

# Design of Pattern Classifiers using Optimum-Path Forest with Applications in Image Analysis

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- Our main focus has been on **image analysis**, where samples may be **pixels**, **images**, or image **objects** (e.g., contours, regions).

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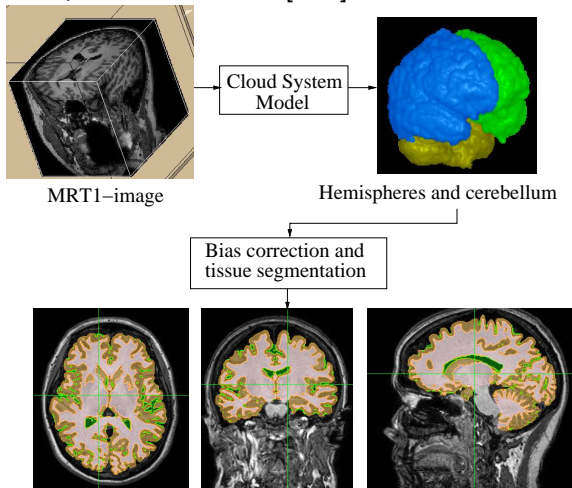


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- a class may consist of multiple clusters.

# Objectives

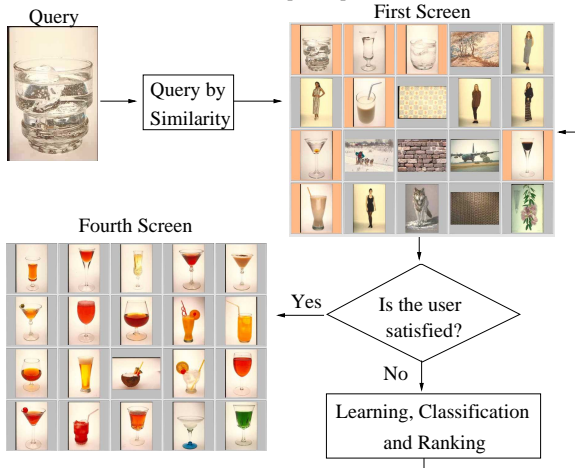
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- Brain tissue segmentation in 3D MR-images [3, 4].
- Content-based image retrieval using relevance feedback [5].

- This methodology can be used for supervised, semi-supervised, and unsupervised learning.

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- The method for brain tissue segmentation is fully automatic, accurate, and one of the fastest approaches to date.
- The method for CBIR can satisfy the user in a few iterations of relevance feedback with significant gain in effectiveness over other state-of-the-art approaches.

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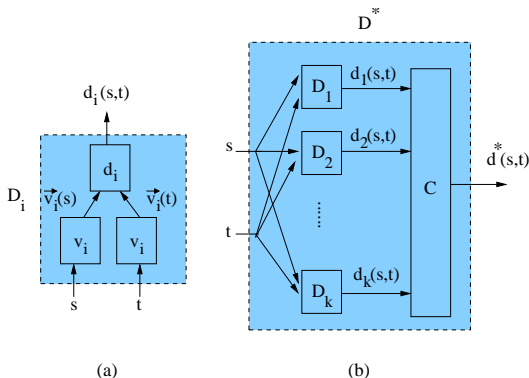
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- Simple descriptors may require more complex distance functions to compare **color** properties [15], **shape** characteristics [16], and **texture** information [17] between samples.

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# Overview

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We have found  $C$  by **genetic programming** [18].

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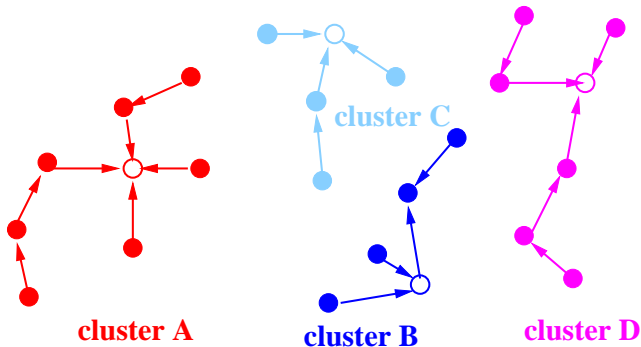
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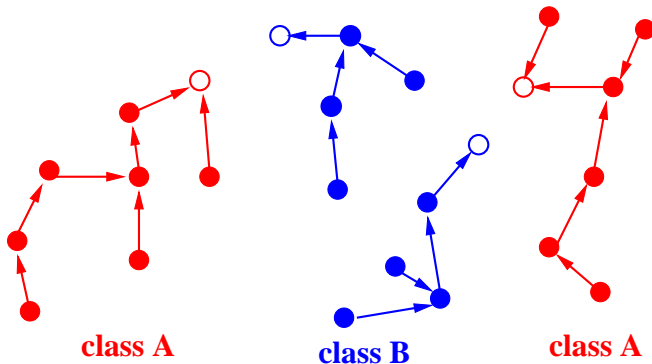
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- The class/cluster label of a new sample  $t \in \mathcal{Z} \setminus \mathcal{T}$  is obtained from  $d^*(s, t)$  using **some samples**  $s \in \mathcal{T}$  and local attributes of the forest [4, 13].

In unsupervised learning, each prototype propagates a distinct **cluster label** to the remaining training nodes of its tree.



Each cluster is one optimum-path tree.

In supervised learning, each prototype propagates its **class label** to the remaining training nodes of its tree.



Each class is one optimum-path forest.

- Training essentially **maximizes** (minimizes) a connectivity map

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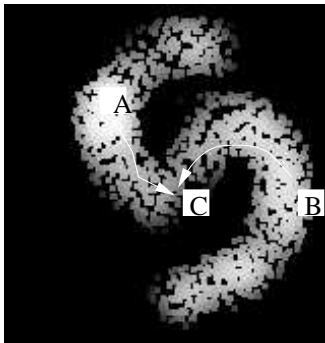
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- The solution is obtained by dynamic programming (i.e., Dijkstra's algorithm extended to multiple sources and more general path-value functions) [19].

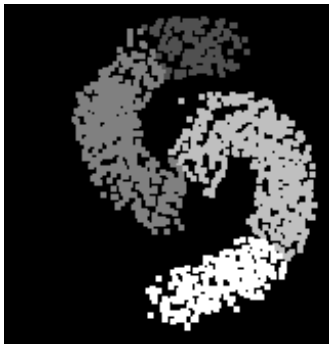
# Unsupervised learning

For clustering, we can estimate a **probability density function (pdf)** and the maxima of the pdf compete with each other, such that each cluster will be an **optimum-path tree** rooted at one maximum of the pdf.



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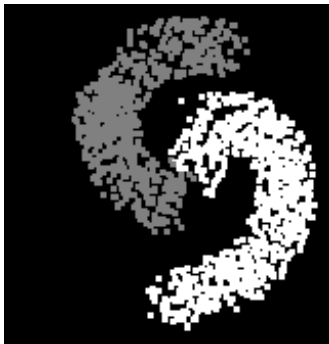
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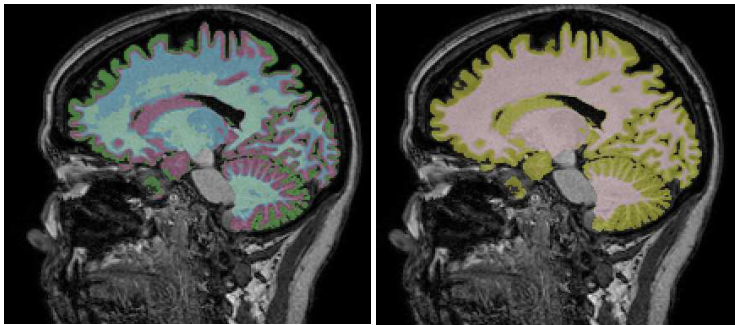
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Prior information is usually required to assign class labels to the clusters.

The unlabeled training samples form a **knn-graph**  $(\mathcal{T}, \mathcal{A}_k)$  with adjacency relation

$\mathcal{A}_k$  :  $(s, t) \in \mathcal{A}_k$  (or  $t \in \mathcal{A}_k(s)$ ) if  $t$  is  $k$  nearest neighbor of  $s$  using the underlying distance space.

The best value of  $k$  is the one whose clustering produces a minimum normalized graph cut in  $(\mathcal{T}, \mathcal{A}_k)$ .

The graph is weighted on the arcs  $(s, t) \in \mathcal{A}_k$  by  $d^*(s, t)$  and on the nodes by the pdf  $\rho(s)$ .

$$\rho(s) = \frac{1}{\sqrt{2\pi\sigma^2}|\mathcal{A}_k(s)|} \sum_{\forall t \in \mathcal{A}_k(s)} \exp\left(\frac{-d^{*2}(s, t)}{2\sigma^2}\right)$$

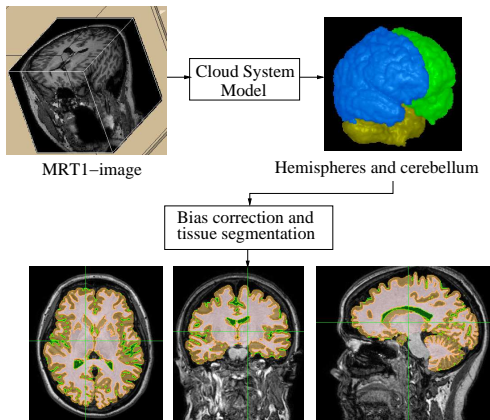
where  $\sigma = \frac{d_f}{3}$  and  $d_f = \max_{(s,t) \in \mathcal{A}_k} \{d^*(s, t)\}$ . The pdf is usually normalized within an interval  $[1, K]$  to facilitate the choice of relevant maxima and extra arcs are added in  $\mathcal{A}_k$  to guarantee arc symmetry on the plateaus of the pdf.

The connectivity map  $V(t)$  is **maximized** for

$$f_{\min}(\langle t \rangle) = \begin{cases} \rho(t) & \text{if } t \in \mathcal{S} \\ \rho(t) - 1 & \text{otherwise} \end{cases}$$
$$f_{\min}(\pi_s \cdot \langle s, t \rangle) = \min\{f_{\min}(\pi_s), \rho(t)\}$$

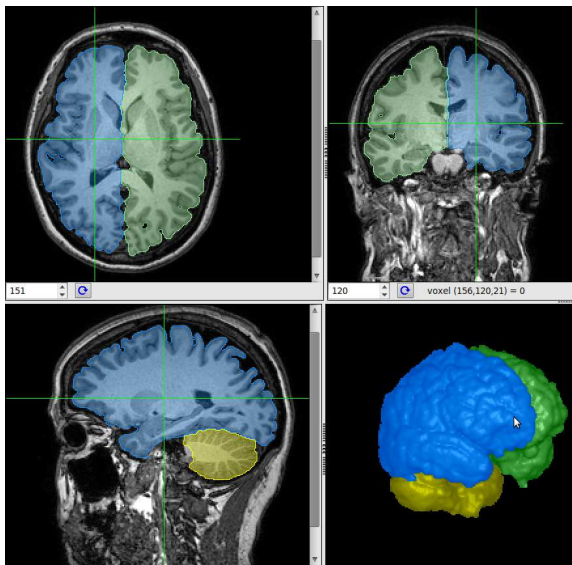
where  $\mathcal{S}$  is the root set (maxima) found on-the-fly.

# Brain tissue segmentation

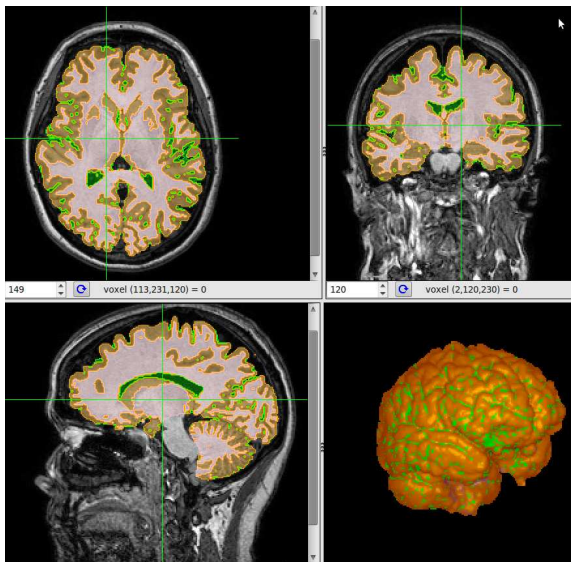


After brain segmentation and bias correction, brain voxels are first classified into CSF or GM+WM and then classified into GM or WM, because the method requires different parameters in each case.

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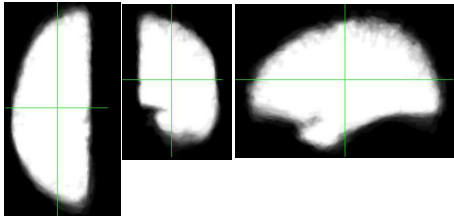
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The method captures possible shape variations and groups them into a few CSMs.

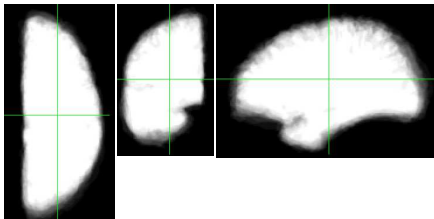
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Orthogonal cuts of the 3D clouds

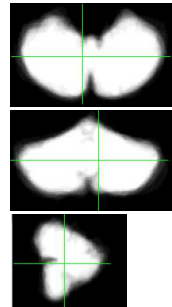
Right Hemisphere



Left Hemisphere

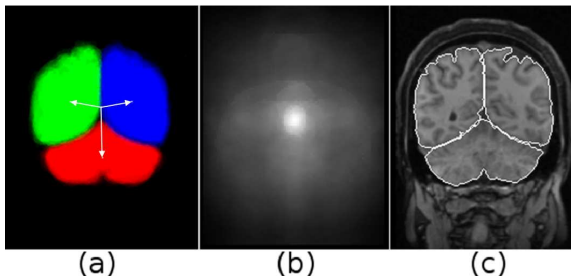


Cerebellum



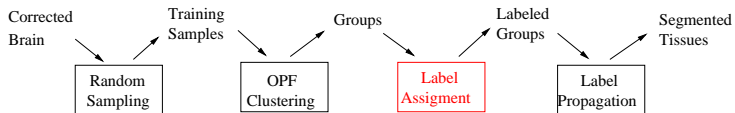
# Brain tissue segmentation

Brain segmentation consists of a **search for the translation** to the image location which produces the highest score, when the reference point of the most suitable CSM is at that position.



We use **four** 3D CSMs for brain segmentation.

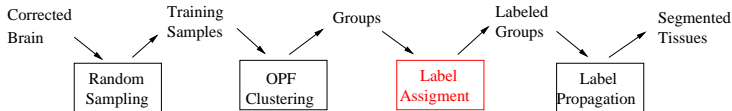
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In each step of voxel clustering.



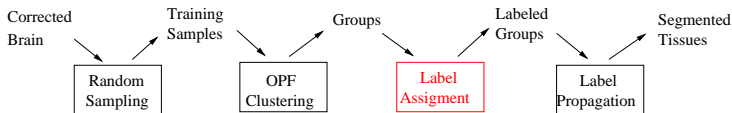
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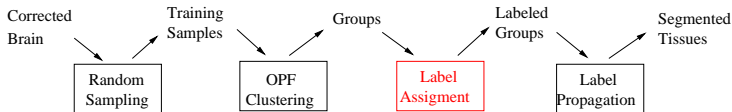
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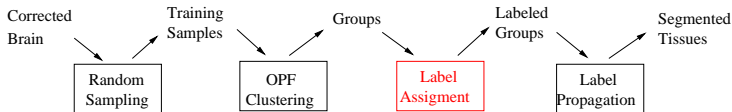
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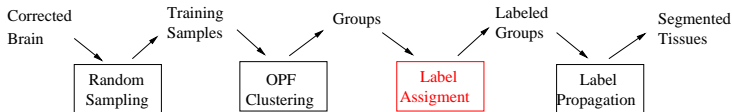
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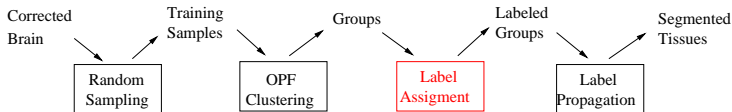
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- A small training set  $\mathcal{T} \subset \mathcal{Z}$  is obtained by **random sampling**.
- The OPF clustering can find groups of voxels in  $\mathcal{T}$ , **mostly from a same class**.

# Brain tissue segmentation



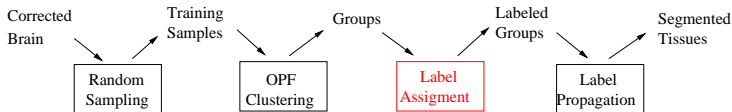
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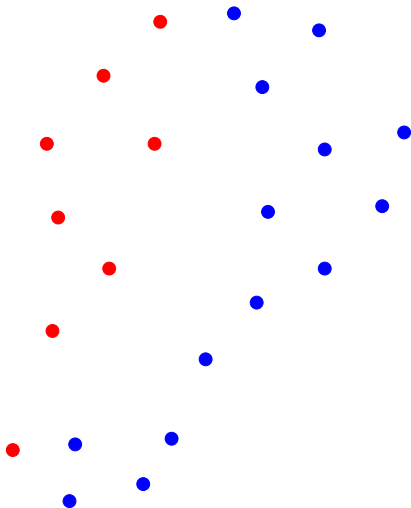
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The entire process takes **less than 2 minutes** in a Core i7 PC, being about 1 minute for brain segmentation using 4 CSMs, and less than 1 minute for bias correction and tissue segmentation.

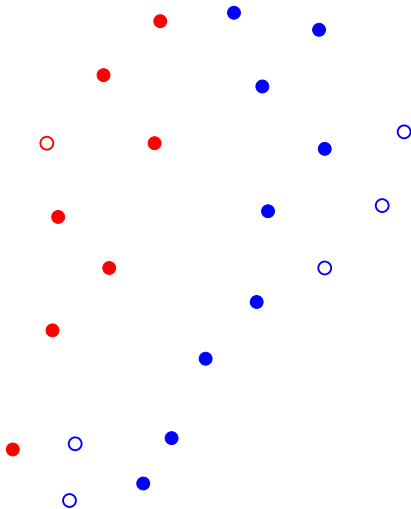
## Dataset



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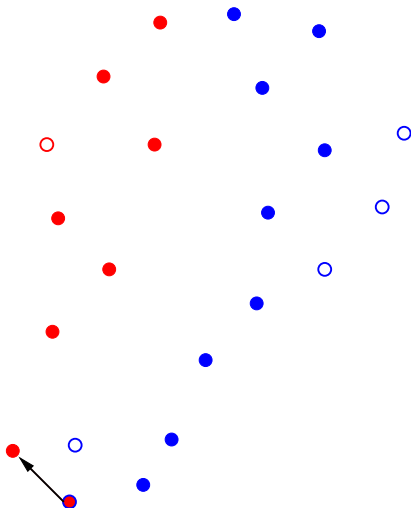


## Training



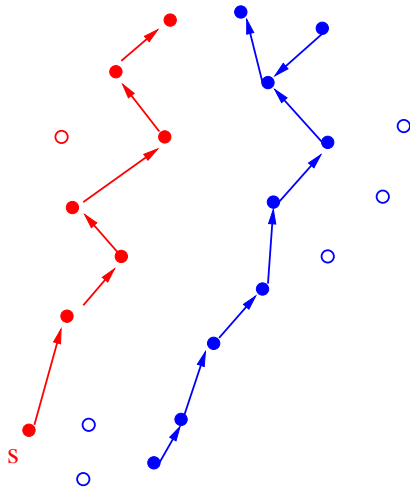
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## 1NN classification



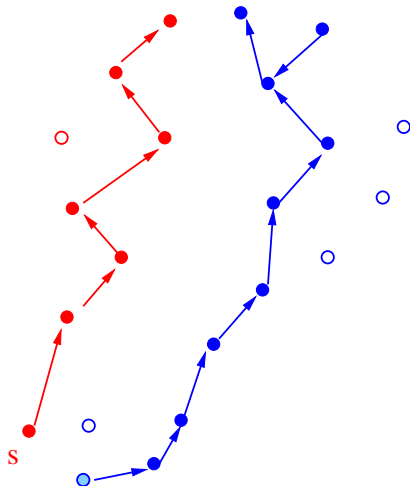
- Consider samples from two classes of a dataset.
- A training set (**filled bullets**) may not represent data distribution.
- Classification by **nearest neighbor** fails, when training samples are close to test samples (**empty bullets**) from other classes.

## OPF training



- We can create an optimum-path forest, where  $V(s)$  is penalized when  $s$  is not closely connected to its class.

## OPF classification



- We can create an optimum-path forest, where  $V(s)$  is penalized when  $s$  is not closely connected to its class.
- $V(s)$  can then be used to reduce the power of  $s$  to classify new samples.

- We interpret  $(\mathcal{T}, \mathcal{A})$  as a **complete graph** with undirected arcs between training samples.

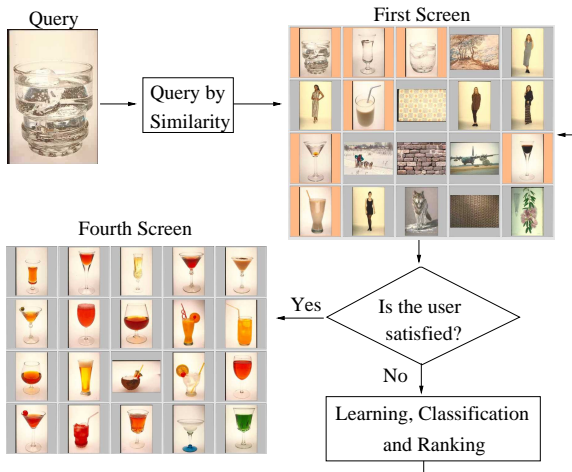
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- The **prototypes** are estimated as all samples that share an arc between **distinct classes** in a minimum-spanning tree of  $(\mathcal{T}, \mathcal{A})$ .
- For a given set  $\mathcal{S} \subset \mathcal{T}$  of prototypes from all classes, the connectivity map  $V(t)$  is **minimized** for

$$\begin{aligned} f_{\max}(\langle t \rangle) &= \begin{cases} 0 & \text{if } t \in \mathcal{S} \\ +\infty & \text{otherwise} \end{cases} \\ f_{\max}(\pi_s \cdot \langle s, t \rangle) &= \max\{f_{\max}(\pi_s), d^*(s, t)\} \end{aligned}$$

where  $d^*(s, t)$  is the distance between  $s$  and  $t$ .

# Content-based image retrieval



The relevant and irrelevant images are the nodes of  $(\mathcal{T}, \mathcal{A})$ , whose arcs are weighted by a color descriptor [15].



# Content-based image retrieval

In each iteration of relevance feedback.

- The training set  $\mathcal{T}$  increases with new relevant (irrelevant) images as indicated by the user.

# Content-based image retrieval

In each iteration of relevance feedback.

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- The relevant candidates are ordered based on their average distances to the **relevant prototypes**.

Show software.

# Dealing with large training sets

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- We have recently devised a method that learns a minimum size of  $\mathcal{T}^*$  in order to obtain a desired classification accuracy on  $\mathcal{T} \setminus \mathcal{T}^*$ .

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- The C source code is available in [www.ic.unicamp.br/~afalcao/libopf](http://www.ic.unicamp.br/~afalcao/libopf).

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